

Drug delivery by phospholipase A₂ degradable liposomes[☆]

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Abstract

The effect of poly(ethylene glycol)-phospholipid (PE-PEG) lipopolymers on phospholipase A₂ (PLA₂) hydrolysis of liposomes composed of stearyl-oleoylphosphatidylcholine (SOPC) was investigated. The PLA₂ lag-time, which is inversely related to the enzymatic activity, was determined by fluorescence, and the zeta-potentials of the liposomes were measured as a function of PE-PEG lipopolymer concentration. A significant decrease in the lag-time, and hence an increase in enzymatic activity, was observed with increasing amounts of the negatively charged PE-PEG lipopolymers incorporated into the SOPC liposomes. The enhancement of the PLA₂ enzymatic activity might involve a stronger PLA₂ binding affinity towards the negatively charged and polymer covered PEG liposomes. © 2001 Elsevier Science B.V. All rights reserved.

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Drug-delivery systems based on liposomes incorporated with polyethylene glycol (PEG)-linked lipids are effective microcarrier system that can retain encapsulated drug, evade rapid clearance from the circulation, and passively target the interstitial tissue of solid tumors (Needham, 1999). However, the final challenges for effective liposomal drug delivery consists of controlling the destabilization, release and absorption of drug at the target site, e.g. in the interstitial tumor tissue.

Different strategies for controlling and obtaining a burst drug release have been developed, including release triggered by the use of environmental-sensitive liposomes that respond to changes in pH (Conner et al., 1984) and release triggered by local intervention techniques such as hyperthermia (Yatvin et al., 1978; Needham et al., 2000).

Another strategy for controlled release and absorption takes advantages of endogenous phospholipases, e.g. phospholipase A₂ (PLA₂), which is found in elevated concentrations in various types of cancer (Abe et al., 1997). PLA₂ catalyzes the hydrolysis of the ester linkage of the *sn*-2 acyl chain of phospholipids, yielding free fatty acids and 1-acyl-lysophospholipids. The overall activity

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of PLA₂ depends strongly on the physical state and the microstructure of the liposome, which are determined by the lipid composition of the membrane (Burack et al., 1993; Hønger et al., 1996; Mouritsen and Jørgensen, 1998). It has been shown that it is possible to control and enhance the hydrolytic activity of PLA₂ by incorporation of submicellar concentrations of (PEG)-linked lipids into unilamellar dipalmitoylphosphatidylcholine (DPPC) liposomes (Vermehren et al., 1998; Jørgensen et al., 1999a,b). PLA₂-triggered release has an additional advantage compared with other triggered release strategies. When the liposomal membrane is destabilized by the action of PLA₂ and the drug is subsequently released, lysolipids and free fatty acids are generated at the same time in locally high concentrations in a one-to-one molar ratio. It is expected that the generated lysolipids and fatty acids act as permeability enhancers and therefore increase drug transport across the biological membrane.

In the present work, we have investigated how incorporation of small concentrations of PEG-linked lipids influences the PLA₂-catalyzed hydrolysis of liposomes composed of stearyl-oleoylphosphatidylcholine (SOPC). Furthermore, we have measured the surface potential (zeta-potential) of the PEG-grafted SOPC liposomes.

Unilamellar fully hydrated liposomes with a narrow size distribution were made from various concentrations of SOPC and Polyethyleneoxide-distearoylphosphatidylethanolamine (DSPE-PEG₇₅₀) (Avanti Polar Lipids, Alabaster, AL) as described by Hope et al. (1985). Purified snake-venom PLA₂ (*Agikistrodon piscivorus piscivorus*) for the lag-time measurements was a gift from R.L. Biltonen, University of Virginia. Assay conditions for the PLA₂ lag-time measurements were 0.15 mM unilamellar liposomes, 150 nM PLA₂, 150 mM KCl, 10 mM HEPES (pH 7.5), 1 mM NaN₃, 30 μM CaCl₂, and 10 μM ethylenediamine tetraacetic acid. The catalytic reaction was initiated by adding 8.9 μl of a 42 μM PLA₂ stock solution to 2.5 ml thermostated liposome suspension equilibrated for at least 20 min at 31°C prior to addition of PLA₂. Zeta-potentials were measured by laser Doppler electrophoresis using a

ZetaMaster (Malvern Instruments Ltd. UK) in the same HEPES buffer (pH 7.5) as used in the PLA₂ lag-time measurements.

Fig. 1 shows the PLA₂ lag-time, τ , as a function of the concentration of DSPE-PEG₇₅₀. The lag-time, which is defined as the time elapsed after addition of the enzyme until the onset of rapid hydrolysis takes place, is determined by a sudden increase in the intrinsic PLA₂ tryptophan fluorescence intensity (Burack et al., 1993). The curve in Fig. 1 shows a decrease in τ , reflecting an enhanced PLA₂ hydrolytic activity when the DSPE-PEG is incorporated into the membrane. The decrease in the lag-time as a function of lipopolymer concentration is in agreement with earlier PLA₂ lag-time measurements on saturated DPPC liposomes incorporated with increasing lipopolymer concentrations (Vermehren et al., 1998; Jørgensen et al., 1999a,b)

Fig. 2 shows the zeta-potential as a function of increasing concentrations of DSPE-PEG₇₅₀. The decrease in the zeta-potential for the PEG-grafted SOPC liposomes correlates with the observed increase in PLA₂ activity reflected as a decrease in the lag-time shown in Fig. 1. It is possible that induction of a negatively charged lipid membrane surface facilitates the binding of PLA₂ and thereby increases the activity of the enzyme. In addition, it is likely that the large hydrophilic polymer headgroup influences the kinetics of the PLA₂ diffusion characteristic close to the lipid

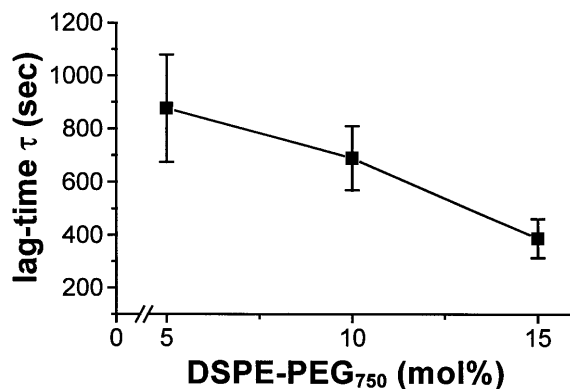


Fig. 1. Phospholipase A₂ (*A. piscivorus piscivorus*) lag-time, τ , of SOPC liposomes as function of DSPE-PEG₇₅₀ lipopolymer concentration obtained at 31°C at pH 7.5.

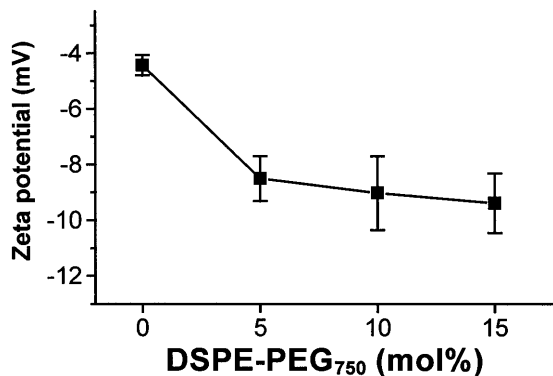


Fig. 2. Zeta-potential of SOPC liposomes as a function of DSPE-PEG₇₅₀ lipopolymer concentration measured in HEPES buffer (pH 7.5).

membrane surface. It has previously been shown that the hydrolytic activity of PLA₂ depends strongly on the physical properties of the lipid membrane substrate (Burack et al., 1993; Burack and Biltonen, 1994; Hønger et al., 1996). Especially, the lateral organization of the lipid membrane is of importance (Hønger et al., 1996, 1997).

The obtained results show that it is possible to control and enhance the hydrolytic activity of PLA₂ towards the polymer-grafted PEG-SOPC liposomes. Furthermore, the advantage of the locally generated permeability enhancers, e.g. lysolipids and free fatty acids, on the transport of the released drug across the target membrane was investigated in a model assay composed of non-hydrolyzable etherlipid liposomes with encapsulated calcein in a self-quenching concentration. The assay measured the permeability enhancing effect of the PLA₂-catalyzed hydrolysis products towards a model membrane system (Davidsen et al., unpublished observations). It was found that the non-bilayer forming hydrolysis products induce a rapid increase in the trans-membrane permeability.

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